

Particle Engineering Technologies for Inhalable Biopharmaceuticals

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Use of discrete element modelling in a film coater
to optimize the tablet film -coating process

*Credit: Liang Li, Elise Vaes and Filip Willemse
Pharmaceutical Product Development & Supply, CPDS*

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IPAC-RS Workshop:
Inhaled Biologics: Preparing for
a Future Beyond Small
Molecules

September 4-5, 2024



Outline

- 1 Drying of Biopharmaceuticals**
 - 2 Particle Engineering – Spray- and Freeze-Drying Technologies**
 - 3 Examples of Inhalable**
 - 4 Summary and Q&A**
-

Slides content previously partly presented at: Formulation Delivery 2023.

Drying of Biopharmaceuticals

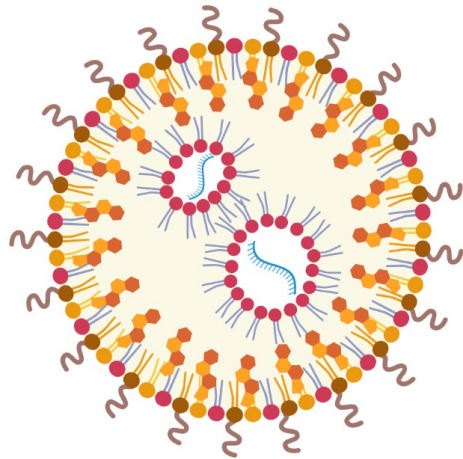
Image: Multiple myeloma illustration

Credit: Johnson & Johnson

Biopharmaceuticals vs. Small Molecules

Biopharmaceuticals

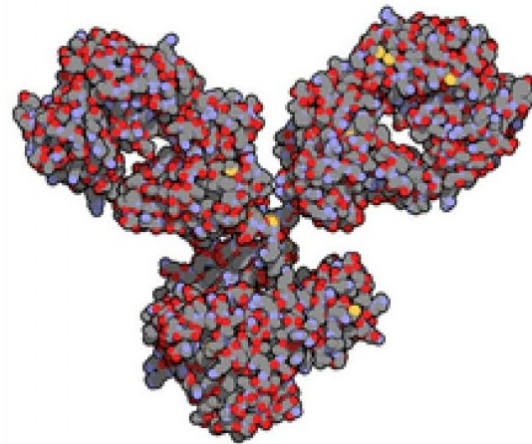
- Produced by a living organism or derived by a living organism by means of recombinant DNA
- High molecular weight (>1 kDa)
- Function depending on 3D-structure
- Proteins, peptides, RNA and DNA, etc.
- Parenteral delivery/sterile



mRNA (280 kDa)

Jung, H.N. et al., "Lipid nanoparticles for delivery of RNA therapeutics: Current status and the role of in-vivo imaging", 2022, Theranostics, 12(17), 7509-7531.

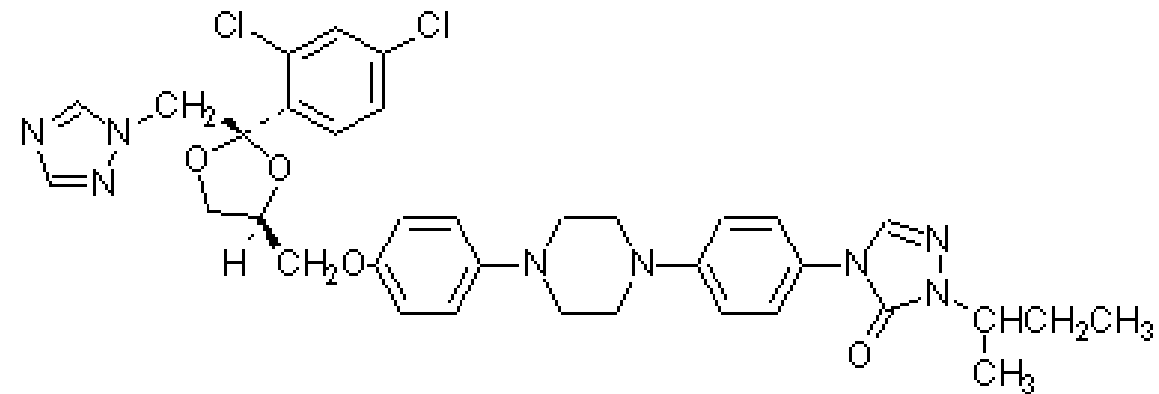
J&J



*Monoclonal AntiBody (mAb)
Infliximab (144 kDa)*

Small Molecules

- Manufactured by controlled and reproducible chemical reactions
- Low molecular weight (<1 kDa)
- Well-defined structure
- Many have low solubility in water
- Oral delivery
- Solid orals, liquid, lyophilized, controlled release (oral and parenteral), inhalation, etc..



Itraconazole (705 Da)

Biomolecules vs. Small Molecules 2

Biomolecules

- Amorphous (typically)
- Highly soluble in water
- *Temperature sensitive*
- High production costs
- Low dose
- Low oral bioavailability
- Parenteral delivery/sterile → **Freeze Drying**



<https://www.jnj.com/hiv>

Small Molecules

- Crystalline (typically)
- Many have low solubility in water
- Post drying necessary
- High dose
- Low production costs
- High oral bioavailability
- Oral delivery → **Spray Drying**



<https://www.jnj.com/healthcare-products>

Lipid Nanoparticles

Nanoparticles recognized as an enabling technology for both small molecules (poorly soluble) and biopharmaceuticals (DNA, mRNA, etc.)

Lipid nanoparticles

- Biocompatible
- Biodegradable
- Increased penetration-permeation profile
- Low cytotoxicity
- Increased bioavailability

SLN/NLC formulation

- Solid lipid
- Liquid lipid
- Surfactant
- Drying protectant

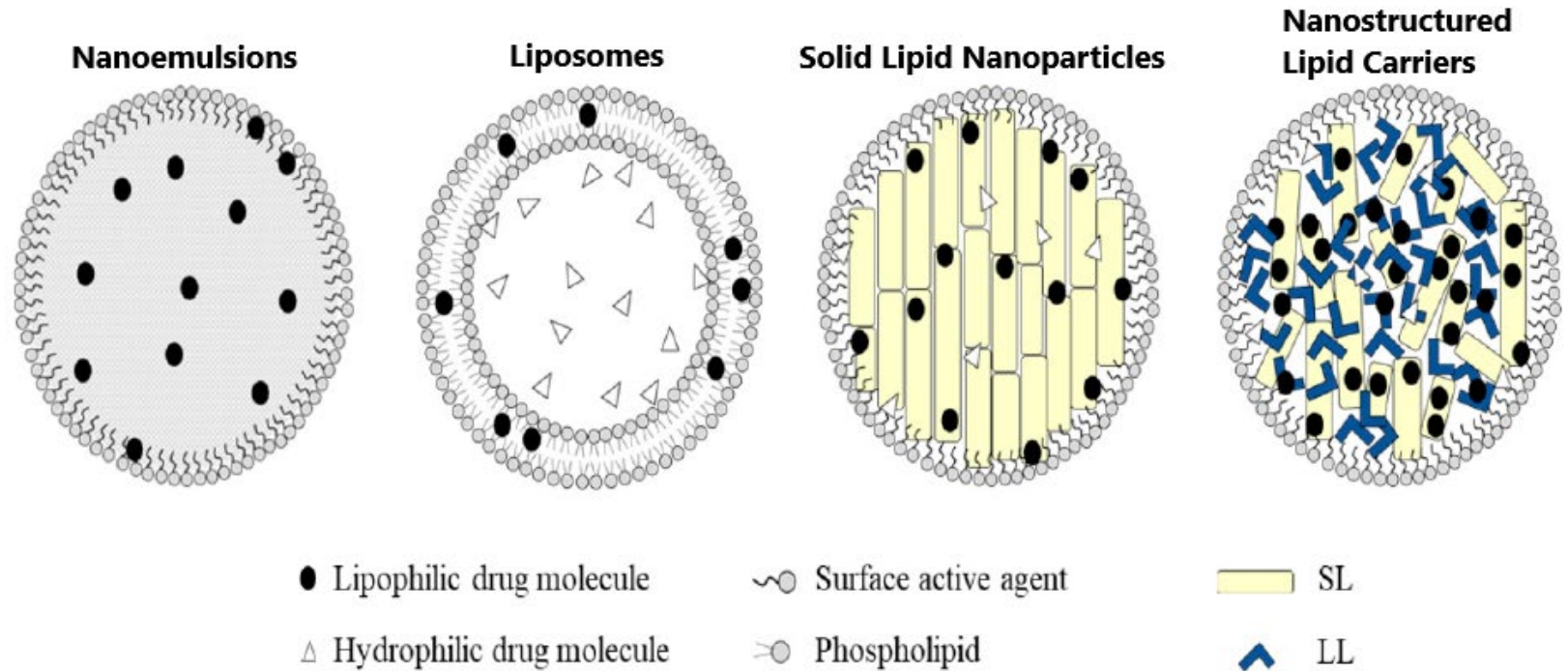


Illustration adapted from Chountoules, M. and Demetrios, C., "Promising Nanotechnology Approaches in Treatment of Autoimmune Diseases of Central Nervous System", 2020, Brain Sci., V10, 338.
Kuentz et al., "Rational Selection of Bio-Enabling Oral Drug Formulations – A PEARL Commentary", 2021, J. Pharm. Sci., V110, pp. 1921-1930.
Hou et al., "Lipid nanoparticles for mRNA delivery", 2021, Nature Reviews, V6, pp. 1078-1094.

Lipid Nanoparticles - Challenges

- Low drug loading
- Drug expulsion
- Stability - Particle size and Polydispersity
- Physical stability - Polymorphic change
- Drug stability

Table 1

Solid lipids used in sustained release drug delivery systems.

Solid Lipids

Lipid excipients	Chemical composition	Properties	Examples	Process
Waxes	Esters of fatty acids and long chain alcohols	Hydrophobic MP = 62–86 °C	Carnauba wax, candelilla wax, rice bran wax, beeswax, solid paraffin (Sasolwax®6403), cetyl palmitate (Precifac®)	Cold, hot
Vegetables oils	Mixture of triglycerides, free fatty acids, phospholipids	Often digestible MP = 60–71 °C	Hydrogenated cottonseed oil (Lubritab®, Sterotex®), hydrogenated soybean oil (Sterotex® K)	Cold, hot
Polyoxylglycerides	Mixture of glycerides and esters of fatty acid and PEG	Partially digestible MP ≈ 50 °C	Stearoyl polyoxyl-6 glycerides (Gelucire® 50/02), stearoyl polyoxyl-32 glycerides (Gelucire® 50/13)	Hot
Fatty acids	Long chain fatty acids	MP = 60–90 °C	Palmitic acid, stearic acid, behenic acid	Cold, hot
Triglycerides	Monoacid triglycerides	MP = 46–73 °C	Glyceryl tripalmitate (Dynasan® 116), Glyceryl tristearate (Dynasan® 118)	Cold, hot
Partial glycerides	Mixtures of mono-, di-, and triglycerides	MP = 54–74 °C	Glyceryl distearate (Precirol® ATO 5), glyceryl monostearate (Myvaplex™ 600; Imwitor®491), glyceryl behenate (Compritol® 888 ATO)	Cold, hot
Fatty alcohol	Mixture of fatty alcohols	MP = 48–56 °C	Cetostearyl alcohol, cetyl alcohol	Cold, hot

Liquid lipids

- Miglyol 8 12 (MCT)
- Kollisolv MCT 70 (MCT)
- Labrafac Lipophile WL 13 4 9
- Oleic Acid
- Squalene

Drying Excipients

- Lactose
- Sucrose
- Trehalose
- Mannitol
- PVP
- L-Leucine
- Dextran

Surfactants

- Polysorbate 80
- Poloxamer 188
- Phosphatidylcholine (soy, egg)
- Poloxamer 407

Table from Rosiaux et al., "Solid lipid excipients—Matrix agents for sustained drug delivery", 2014, J. Cont. Release, V188, pp.18-30.

Doktorovova, S., Shegokar, R. and Souto, E.B., "Role of Excipients in Formulation Development and Biocompatibility of Lipid Nanoparticles (SLNs/NLCs)", 2017, Nanostructures for Novel Therapy, Ch. 30, pp. 811-843.

Salminen et al., "Influence of spray drying on the stability of food-grade solid lipid nanoparticles", 2019, Food Res. Int., V119, pp. 741-750

Drying of Pharmaceuticals – Potential Approaches

Drying of Pharmaceuticals – Why?

- Pharmaceuticals are more stable in the solid state
- Reduction of transportation costs
- Ease of handling and storage

Spray Drying

- *Investment/Operating costs: 5-8 times lower than FD*
- Organic solvents feasible
- High capacity & Continuous Process
- Particle Engineering
- PAT might be applied

Freeze Drying

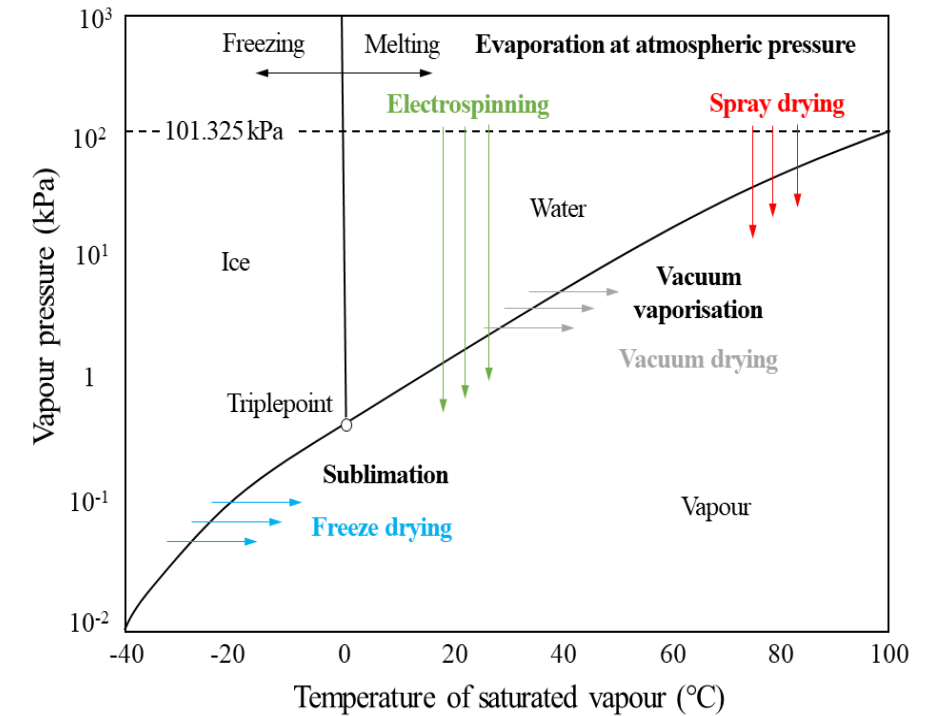
- Injectables/Parenterals
- Sterile manufacturing
- High yields
- Small volumes

Spray Drying feasible for:

- Powder properties important for functionality e.g. Oral Dosage Forms, **Inhalable Particles**
- Large volumes
- Low/Medium Heat sensitive products

Freeze Drying feasible for:

- **Injectables/Parenterals/Sterile products**
- **Small volumes**
- **Heat sensitive products**



Vass et al., "Drying Technology Strategies for Colon-Targeted Oral Delivery of Biopharmaceuticals", 2019, J. Cont. Rel., Vol. 296, pp.162-178.
Walton and Mumford, 1999, "Spray Dried Products – Characterization of Particle Morphology", Trans IChemE, V77, pp. 21-38.

Particle Engineering using Spray- and FreezeDrying Technologies

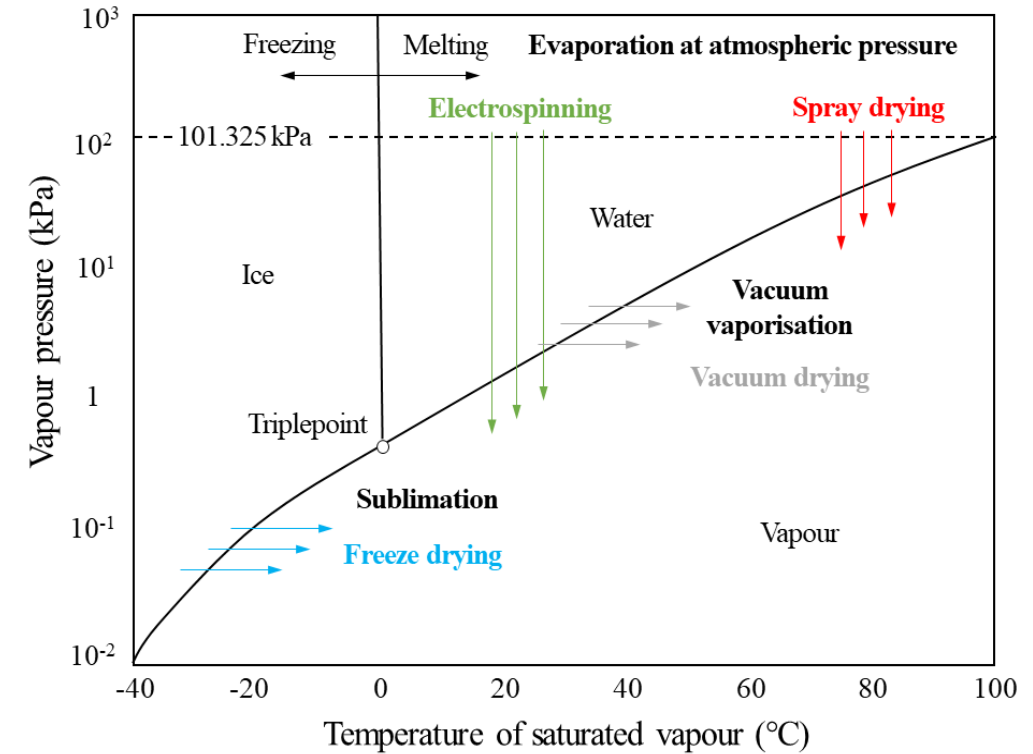
Image: Multiple myeloma illustration

Credit: Johnson & Johnson

Drying Processes for Inhalable Biopharmaceuticals

Drying ± Milling (+ Powder Filling)

1. Spray Drying
2. Electro-spraying/-spinning + Milling (spinning)
3. Spray-Freeze Drying
4. Supercritical Drying
5. Continuous Bulk Freeze Drying + Milling
6. Active Freeze Drying + Milling
7. Thin Film Freeze Drying
8. Drying (particles) + Atomic Layer Deposition
9.



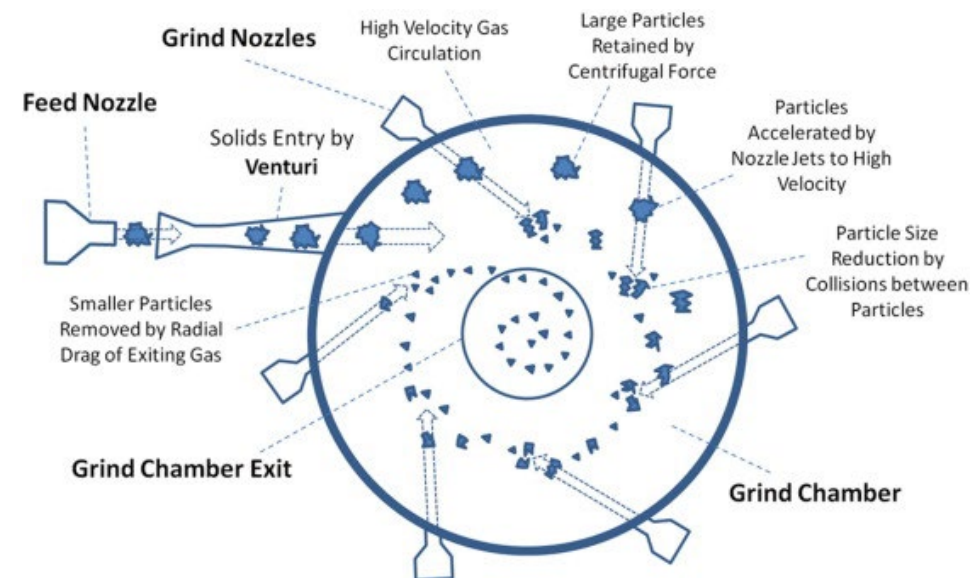
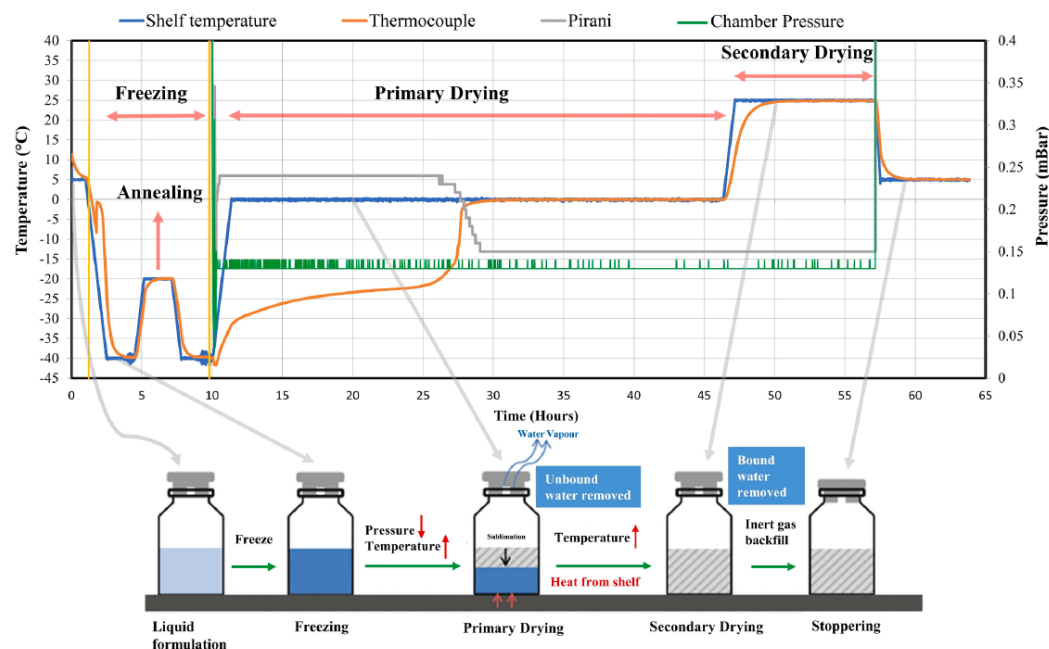
Walters et al, 2014, "Next Generation Drying Technologies for Pharmaceutical Applications", J. Pharm Sci., V103, pp. 2673-2695.

Vass et al, 2019, "Drying Technology Strategies for Colon-Targeted Oral Delivery of Biopharmaceuticals", J. Cont. Rel., Vol. 296, pp.162-178.

Sharma et al, 2021, "Innovative Drying Technologies for Biopharmaceuticals", Int. J. Pharm., V609, Article 121115.

Samborska et al, 2022, "Innovations in spray drying processes for food and pharma industries", J. Food Eng., V321, Article 110960.

Freeze Drying + Jet Milling



■ Advantages

- + Low temperature drying
- + High yield
- + Sterile manufacturing (*Pharma*)
- + Preservation of shape (*Food*)

■ Challenges

- Long drying times
- Expensive
- *Difficult to scale -up*
- Stresses during freeze drying (freezing and dehydration) and milling (mechanical)

Sharma et al., 2021, "Innovative Drying Technologies for Biopharmaceuticals", Int. J. Pharm., Vol. 609, Article 121115.

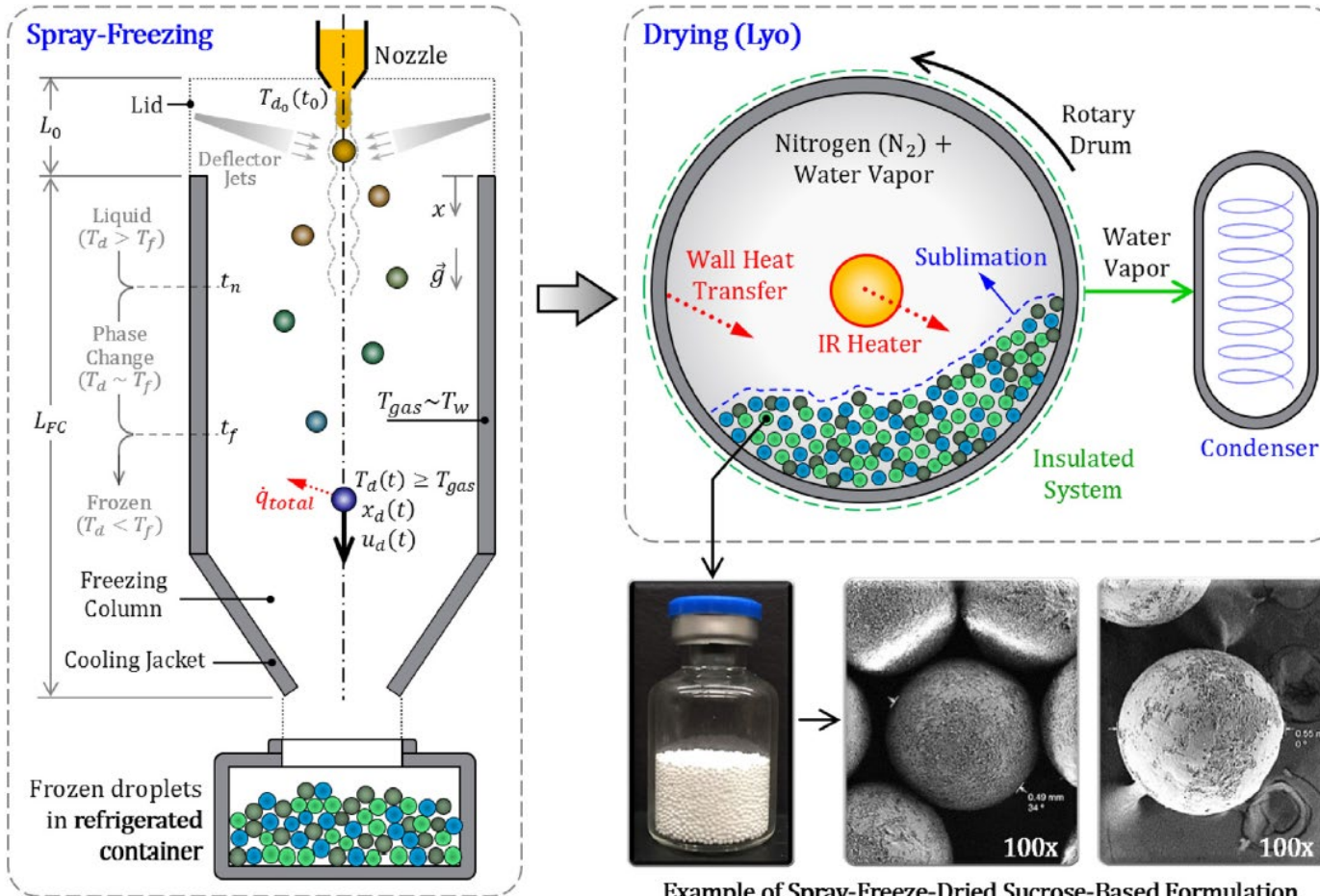
C. Ratti, 2013, "Freeze drying for food powder production", in Handbook of Food Powders, Woodhead Publishing, DOI : 10.1533/9780857098672.1.57, pp. 57-84.

Yang et al., 2024, "Characterization and biological activity evaluation of water-soluble resveratrol complexes obtained by spray drying, ball milling and jet milling", J. Drug Del. Sci. Tech. V100, doi.org/10.1016/j.jddst.2024.106075.

Macdonald et al., 2016, "The spiral jet mill cut size equation", Powder Tech. V299, pp. 26-40, dx.doi.org/10.1016/j.powtec.2016.05.016.

Spray-Freeze Drying

"2-step production of a dry powder by 1) Atomization of a liquid into droplets and freezing the droplets by a cold gas, liquid or surface, and 2) freeze drying the frozen particles"

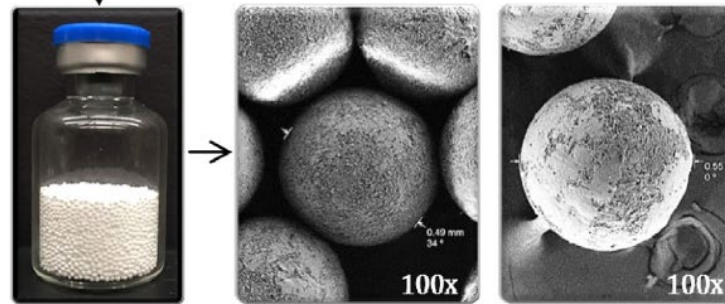


Advantages

- + Ideal for heat sensitive proteins
- + High yield

Challenges

- Scale-up challenging
- Capacity
- Freezing and dehydration stresses



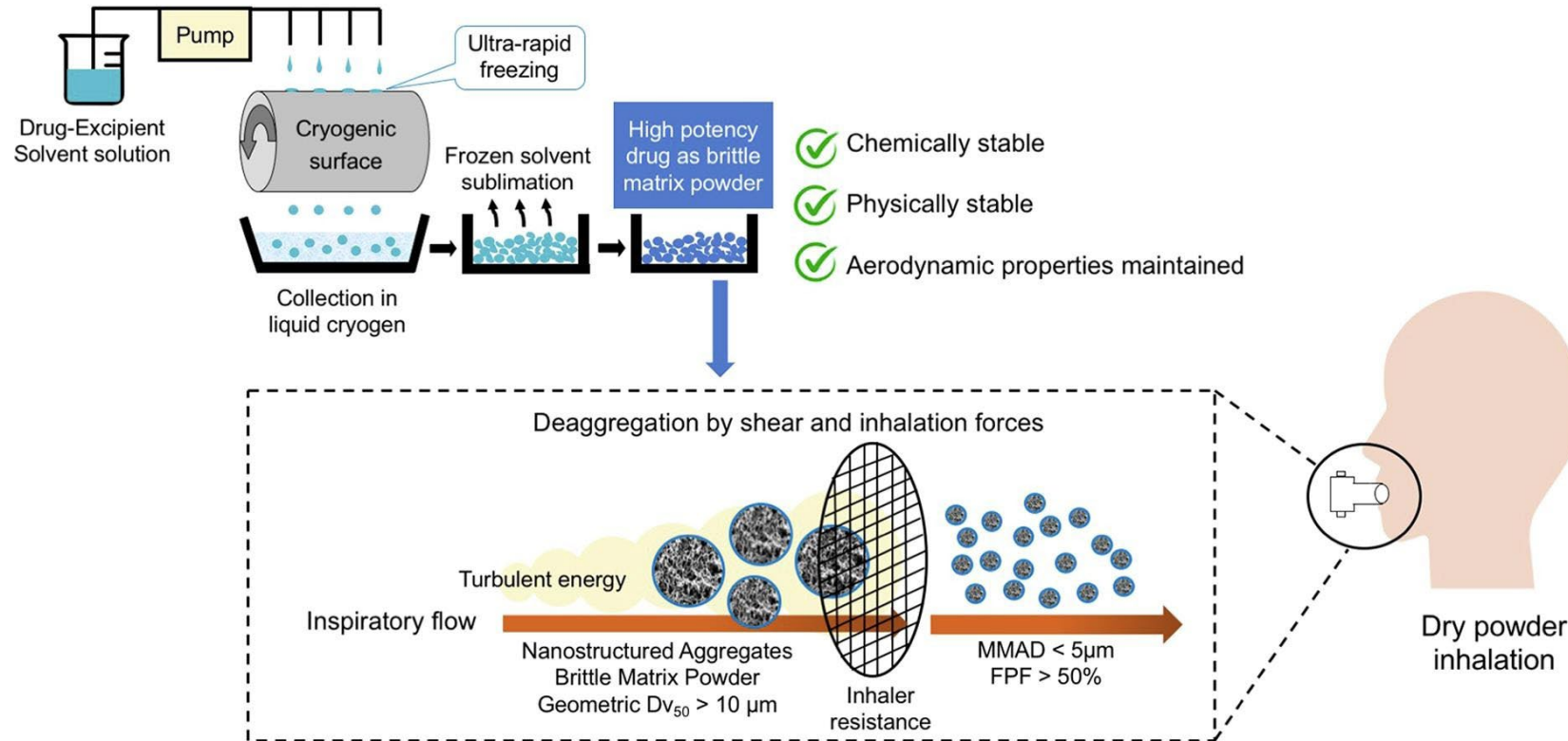
Example of Spray-Freeze-Dried Sucrose-Based Formulation

I.B. Sebastiao et al., 2019, "Bulk Dynamic Spray Freeze-Drying Part 2 - Model-Based Parametric Study for Spray-Freezing Process Characterization", J. Pharm Sci., Vol. 108, pp.2075-2085.

Chang et al., 2021, "Dry powder pharmaceutical biologics for inhalation therapy", Adv. Drug Del. Reviews, V172, pp. 64-79.

Farinha et al., 2023, "Spray Freeze Drying of Biologics: A Review and Applications for Inhalation Delivery", Pharm. Res., V40, doi.org/10.1007/s11095-022-03442-4.

Thin-Film Freeze-Drying Technology for Inhalation



Advantages

- + Ideal for heat sensitive proteins
- + Minimal air/water interface

Challenges

- High specific surface area
- Low density particle
- Freezing and dehydration stress

Atomic Layer Deposition

- Technology from the semiconductor industry
 - Layer is well-controllable in nm-size range
 - Nonconformal object are uniformly coated
- Idea/Purpose:
 - Improve powder processability (i.e. dispersibility, flowability)
 - Improved stability against water and oxygen

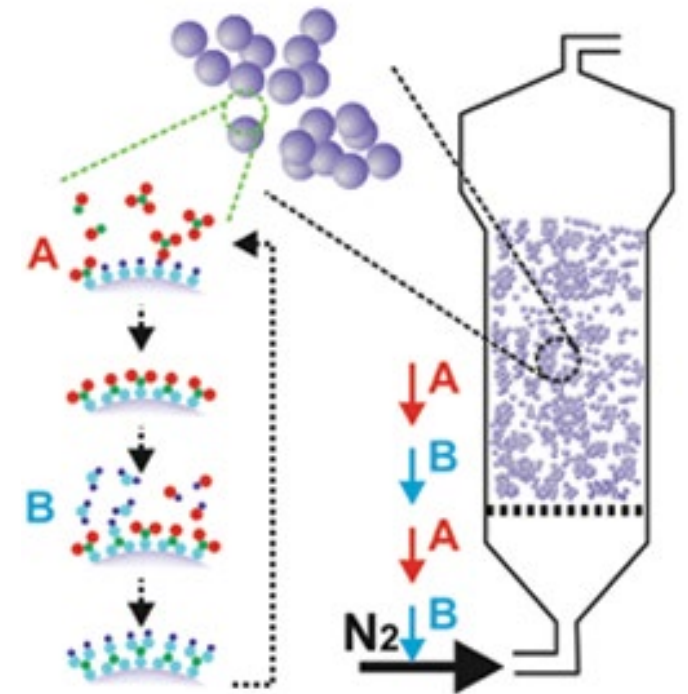
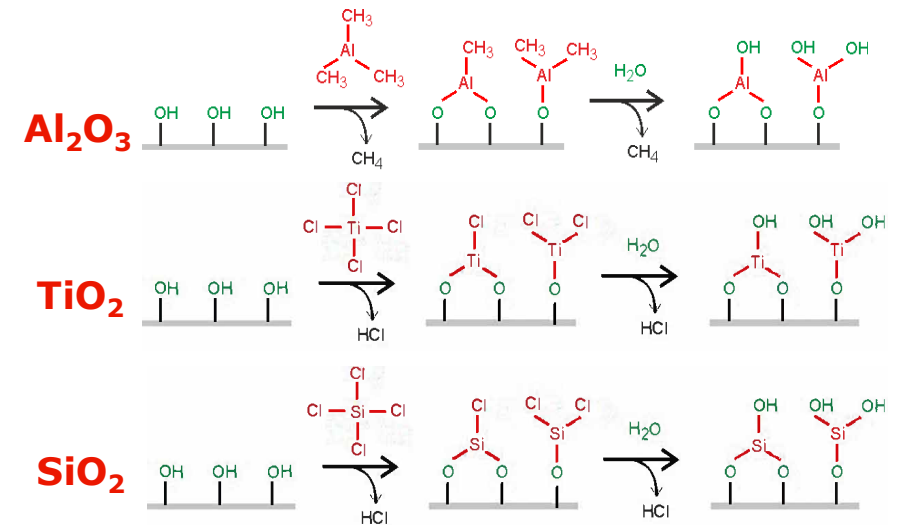
Advantages

- + Improved dispersibility and flowability
- + Small excipient amount (typically 1-5 wt.%)

Challenges

- New technology (supplier, benefits, ...)
- *Mainly metaloxides as coatings*
- Toxicology
-

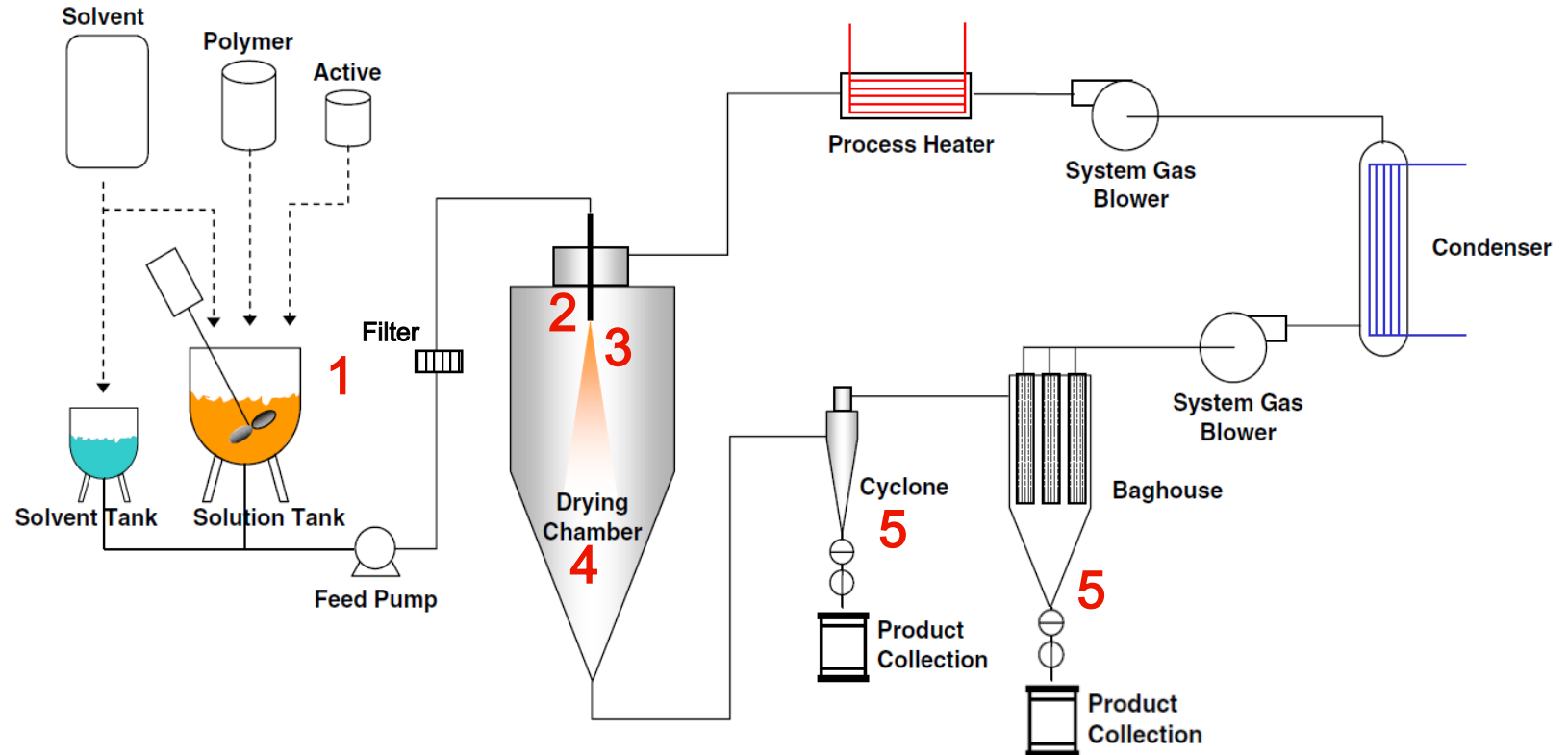
La Zara et al., 2021, "Controlled Pulmonary Delivery of CarrierFree Budesonide Dry Powder by Atomic Layer Deposition", ACS Nano, V15, doi.org/10.1021/acsnano.0c10040.
 R. van Ommen, 2020, "ALD on particles - Scalable production of nanostructured materials", NEVAC Blad, 58(2); https://nevac.nl/archief_pdf/pdf_194.pdf.



Spray Drying – Concept & Elements

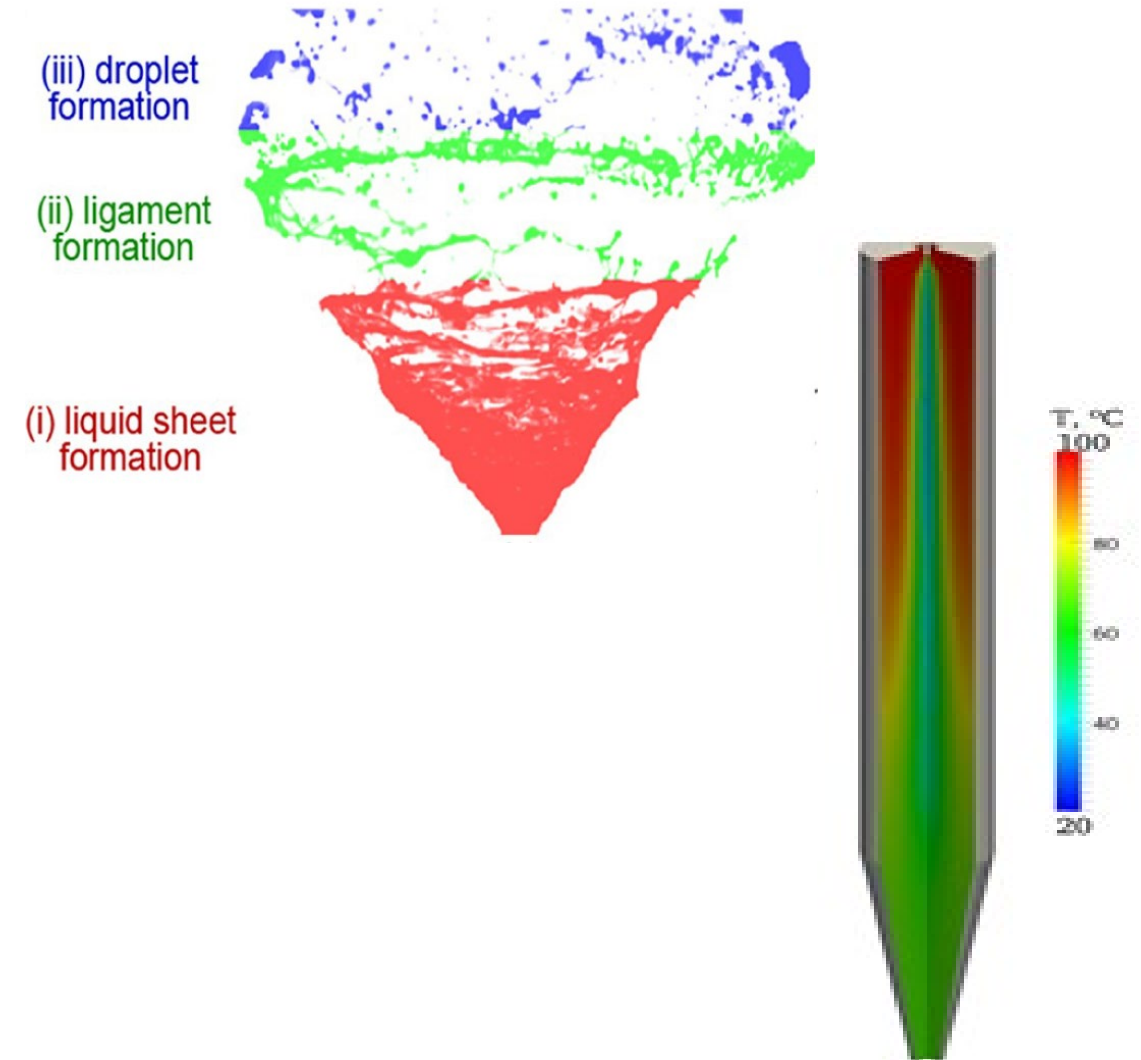
"1-step production of a dry powder by atomization of a liquid into droplets with simultaneous exposure to a hot gas, whereby the liquid is evaporated"

1. Solution Preparation including Filtration
2. Atomization
3. Mixing of droplets and the drying gas
4. Drying
 - Inlet 80-200 °C
 - Outlet 30-80 °C
5. Separation of particles and gas



Stresses in Spray Drying

- **Atomization stresses:**
 - Shear forces
- **Thermal stresses:**
 - Inlet & outlet temperature
 - Residence time
 - Formulation (proteins at the Air-Water interface)
- **Powder recovery system:**
 - Temperature
 - Humidity
 - Residence time



CFD simulation shown courtesy
Hovione FarmaCiencia S.A.

Atomization illustration from Shrestha et al., "Primary break-up and atomization characteristics of a nasal spray", 2020, PLOS ONE., V15(8):e0236063.

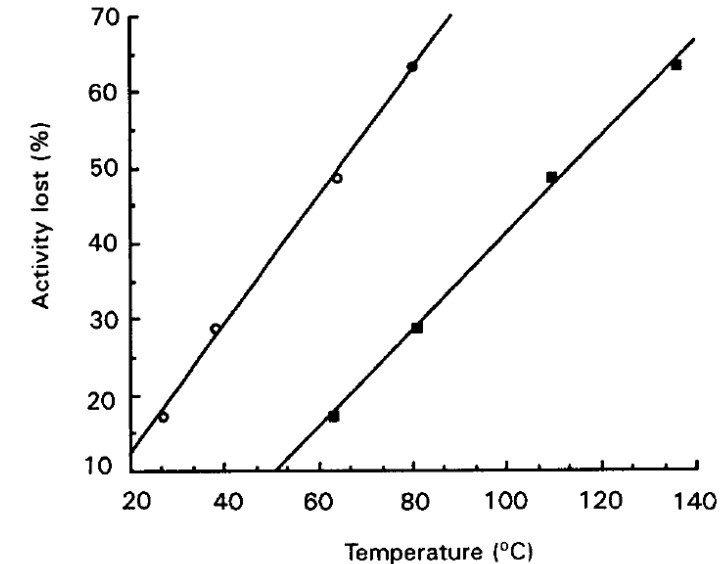
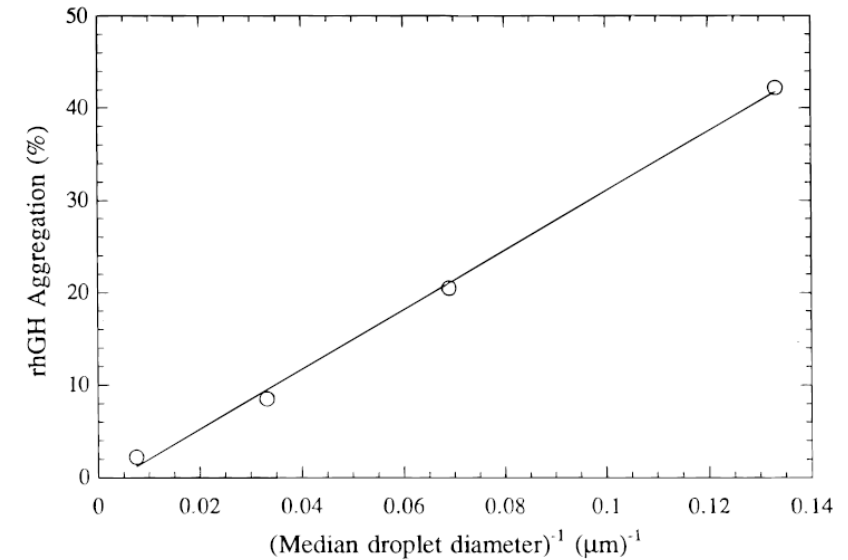
Degradation Examples

■ Human Growth Hormone

- Degradation by Air-Water interface exposure i.e. high atomization force (small droplets)
- Degradation reduced by use of surfactant (Tween20)

■ β -Galactosidase

- Degradation by temperature (same atomization conditions)
- Degradation reduced by use of excipients (Sucrose, Trehalose)



Broadhead et al., "The effect of process and formulation variables on the properties of spray dried β -galactosidase", J. Pharmacy and Pharmacology, 1994, V46, pp. 458-467.

Mumenthaler et al., "Feasibility study on spray-drying protein pharmaceuticals: recombinant human growth hormone and tissue-type plasminogen activator", 1994, Pharm. Res. V11, pp. 12-20

Maa et al., "Spray-Drying of Air-Liquid Interface Sensitive Recombinant Human Growth Hormone", 1998, J. Pharm. Sci., V87(2), pp. 152-159.

Spray Drying Quality-by-Design – Prior Knowledge, Impact on CQA's, and Critical Process Parameters

1. **Formulation** impacts physical and chemical properties
 - Concentration, Viscosity and Solvent(s) choice, Polymer type, API:polymer (sugar) ratio
 - Viscosity: Atomizer type & Droplet size
2. **Atomisation** (droplet size) impacts primarily Particle Size and Solvent Cont.
 - Specific atomizer design
 - *2-Fluid Nozzle*: Liquid & Atomisation Gas flow rate, Ratio between flow rates
 - *Pressure Nozzle*: Pressure (Liquid flow rate)
3. **Droplet -Gas Contact** impacts primarily Morphology and Density
 - Drying Gas flow rate
 - Gas disperser design (fixed)

4. **Drying** impacts Solvent Cont., Activity, Purity, HMWP, T_g
 - Drying Gas flow rate
 - Inlet temperature
 - Liquid flow rate
 - Condenser temperature
 - Outlet temperature = func. (Inlet T, Liquid flow rate, Drying gas flow rate, Condenser T and Liquid properties)
 - Relative Saturation = func. (Inlet T, Liquid flow rate, Drying gas flow rate, Condenser T and Liquid properties)
5. **Collection** impacts Solvent Cont., Activity, Purity, HMWP, T_g
 - Collector design: Cyclone vs. Bag-filter
 - Residence time
6. **Post Drying** impact Solvent Cont.
 - Temperature
 - Time

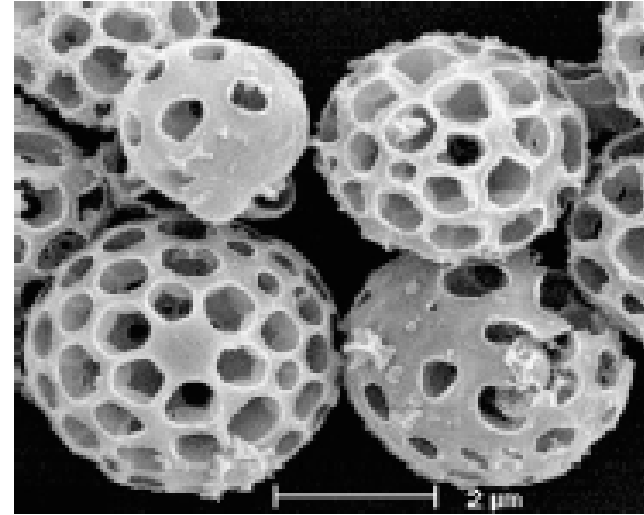
Formulation, Process Understanding and CQAs

Process understanding – Spray Drying & Formulation:

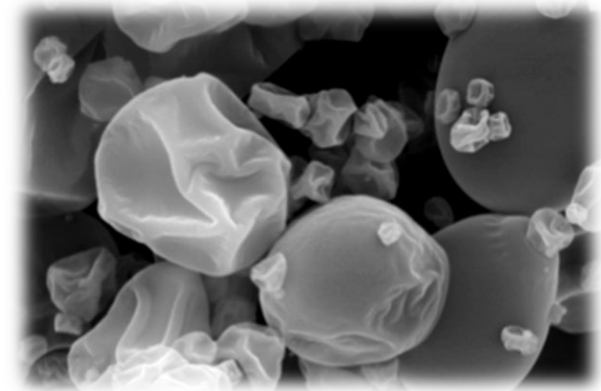
- Impact of spray drying parameters on the Critical Quality Attributes (CQAs)
- Interaction between process parameters
 - E.g. through Design-of-Experiments (DoE)
- Critical Material Attributes impact on CQAs
 - Solution composition (solvents)
 - Excipients (polymers, sugars)
 - Surfactants

Typical Critical Quality Attributes:

- Impurity profile / High Molecular Weight Protein
- Residual Solvent
- Particle size
- Powder density
- Flowability (*inc. with particle size and density*)
- Particle shape (inhalation)
- API form (crystalline vs. amorphous)
- Yield (process quality attribute)



Pulmospheres™
Vehring, R. "Pharmaceutical Particle Engineering via Spray Drying", 2008,
DOI: 10.1007/s11095-007-9475-1.



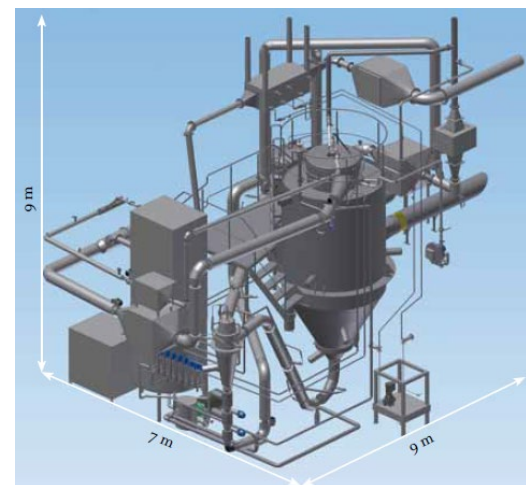
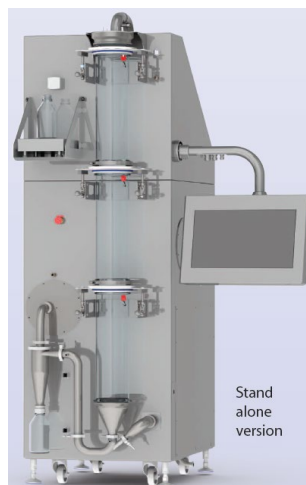
The strategy for scaling up a spray drying process will depend on the specific product:

- | | |
|---------------------|------------------------------------|
| ▪ Pulmonary | Particle size maintained |
| ▪ Solid Dosage Form | Increase particle size/flowability |

Spray Drying Platforms- Inhalation

Spray Dryer Size	Drying Gas Flow Rate	Powder Production Rate ¹	Residence Time	Particle Size (D_{v50})	Yield	
					Cyclone	Bag Filter
Lab (Buchi)	30 kg N ₂ /h	0.005 kg/h	2 s	2 – 15 μ m	50-90%	NA
Lab (ProCepT)	30 kg N ₂ /h	0.005 kg/h	5 s	2 – 50 μ m	50-90%	NA
Small Pilot/Commercial (PSD-1)	100 kg N ₂ /h	0.05 kg/h	25 s	2 – 40 μ m	40-80%	≥80%
Commercial (PSD-4)	1.250 kg N ₂ /h	1 kg/h	45 s	2 – 120 μ m	40-80%	≥80%
Commercial XL (PSD-7)	10.000 kg N ₂ /h	8 kg/h	45 s	2 – 120 μ m	40-80%	≥80%

¹2 wt.% aqueous solution



Examples of Inhalable Biopharmaceuticals

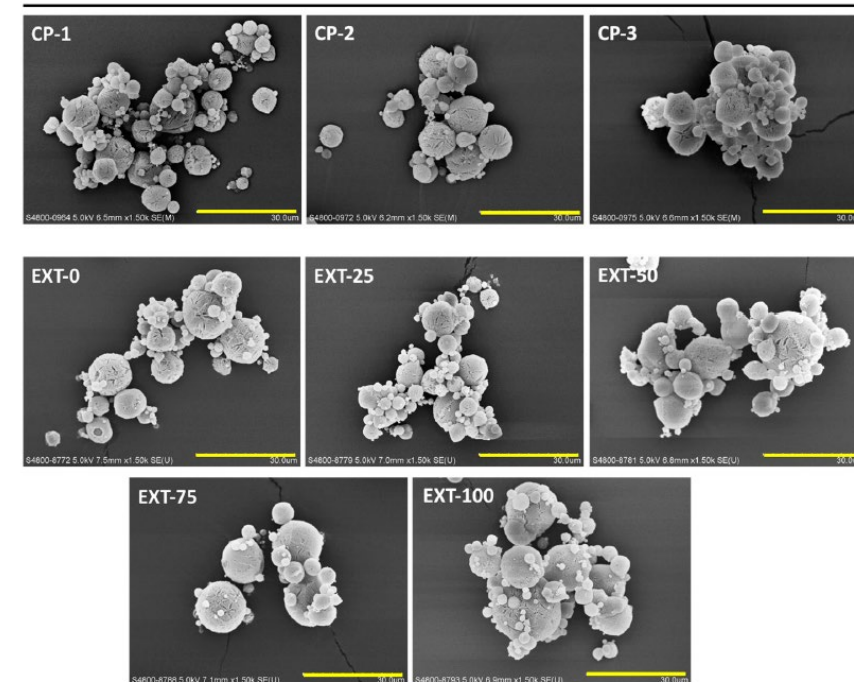
Image: Multiple myeloma illustration

Credit: Johnson & Johnson

Spray-Freeze Drying of BSA with HP- β -CD

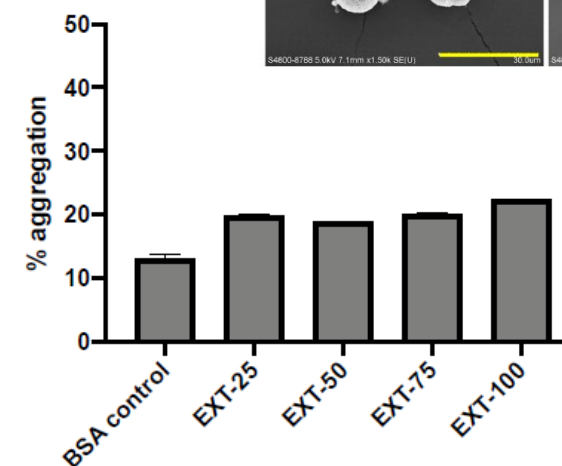
- BSA protein with HP- β -CD
- 5 wt.% total solids in water
- **Spray-Freeze Drying: 2-fluid nozzle into liquid nitrogen**
- **Good aerodynamic properties, but BSA aggregation**
- **Atomization gas flow rate critical for aerodynamic properties and aggregation**

6% BSA, 5% solute concentration, 473 L/h



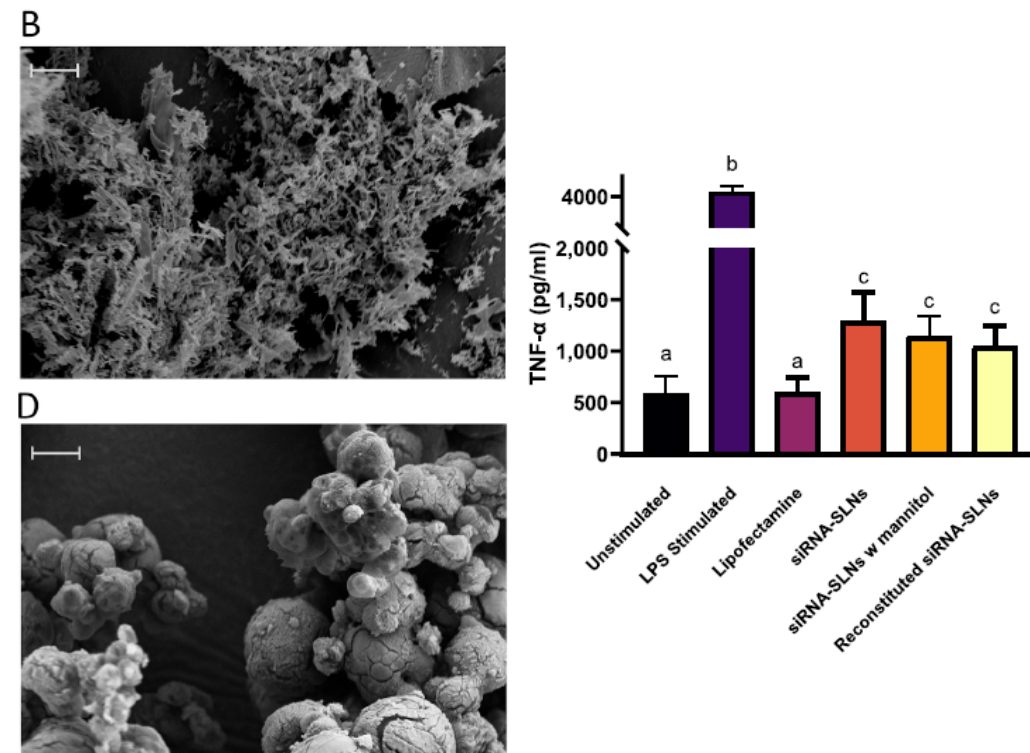
Formulation	Volumetric Diameter				EF (%)	FPF (%)	MMAD (μ m)
	D ₁₀ (μ m)	D ₅₀ (μ m)	D ₉₀ (μ m)	Span			
CP-1	4.3 \pm 0.1	10.8 \pm 0.3	24.7 \pm 1.0	1.9 \pm 0.0	96.5 \pm 0.5	60.4 \pm 6.4	2.1 \pm 0.5
CP-2	4.3 \pm 0.1	10.8 \pm 0.2	24.8 \pm 0.3	1.9 \pm 0.0	95.4 \pm 0.9	59.8 \pm 8.1	2.0 \pm 0.8
CP-3	4.3 \pm 0.0	10.6 \pm 0.1	24.4 \pm 0.3	1.9 \pm 0.0	95.7 \pm 1.1	61.1 \pm 8.7	1.5 \pm 0.2
EXT-0	3.9 \pm 0.1	9.9 \pm 0.3	24.4 \pm 0.9	2.1 \pm 0.0	98.5 \pm 0.6	60.5 \pm 2.7	1.8 \pm 0.2
EXT-25	4.0 \pm 0.0	10.4 \pm 0.2	25.5 \pm 0.5	2.1 \pm 0.0	100 *	65.5 \pm 1.7	1.4 \pm 0.0
EXT-50	4.1 \pm 0.0	11.1 \pm 0.3	27.2 \pm 1.2	2.1 \pm 0.1	100 *	63.6 \pm 1.8	1.4 \pm 0.1
EXT-75	3.9 \pm 0.1	10.8 \pm 0.7	27.2 \pm 1.9	2.2 \pm 0.0	98.3 \pm 0.7	54.7 \pm 3.3	2.1 \pm 0.3
EXT-100	3.8 \pm 0.0	11.7 \pm 0.5	31.1 \pm 2.0	2.3 \pm 0.1	98.4 \pm 0.4	52.3 \pm 4.7	2.5 \pm 0.6

* The amount of protein in the capsule and inhaler was below the lower limit of the standard curve (i.e., unrecoverable from the capsule and inhaler).



Thin-Film Freeze-Drying of Inhalable SLN with siRNA

- **Formulation:**
 - Lecithin, Cholesterol, Stearoyl Hydrazone PEG, DOTAP, TNF- α siRNA, Mannitol
 - Particle size = 150-200 nm
- **Powders produced by TFFD, Spray Drying, and Freeze Drying**
 - After Freeze Drying SLN particle size not preserved
 - SLN particle size preserved after TFFD and Spray Drying
- TFFD powder had the best aerosolization properties and preserved siRNA functionality



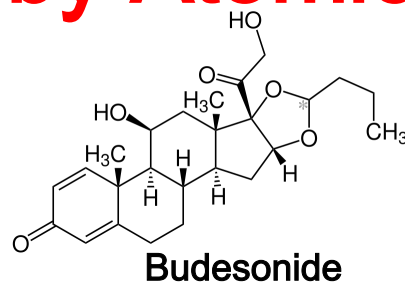
	Spray dried	TFFD	Shelf freeze-dried
Specific surface area (m ² /g)	0.92 ± 0.12	19.34 ± 2.57*	ND
Moisture content (%)	1.17 ± 0.04	0.23 ± 0.07*	0.35 ± 0.12*
FPF%	22.42 ± 12.88	37.01 ± 4.52*	ND
MMAD (μm)	5.97 ± 1.73	3.96 ± 0.97*	ND
GSD	2.30 ± 0.49	3.25 ± 0.61	ND

Wang et al., "Aerosolizable siRNA-encapsulated solid lipid nanoparticles prepared by thin film freeze-drying for potential pulmonary delivery", 2021, Int. J. Pharm., V596, 120215.

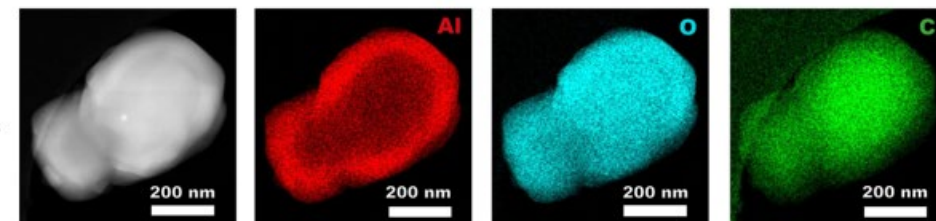
Inhalable Budesonide by Atomic Layer Deposition

- Formulation:**

- Budesonide coated with SiO_2 , TiO_2 and Al_2O_3 with varying thicknesses

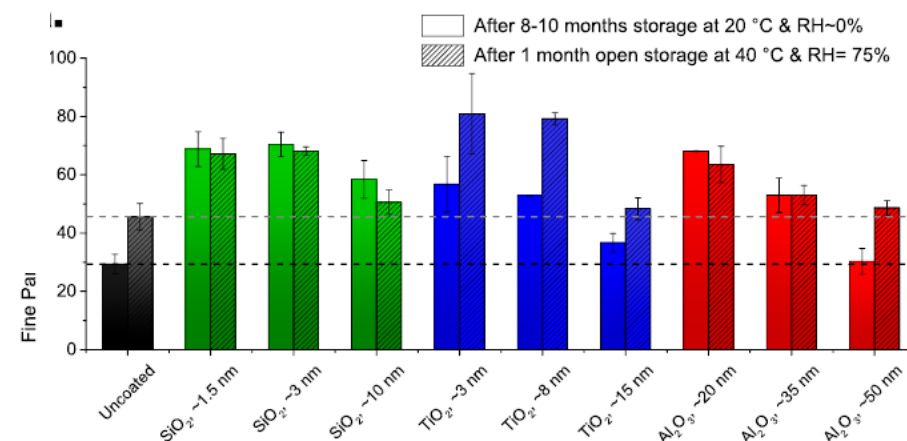
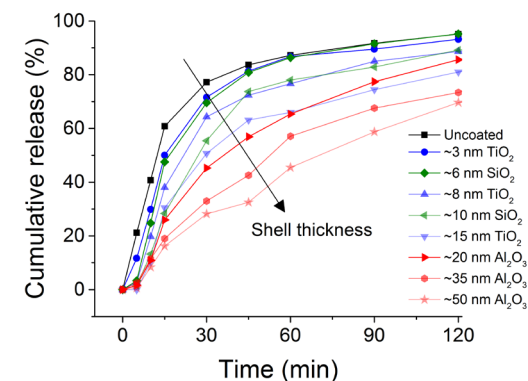


Al_2O_3



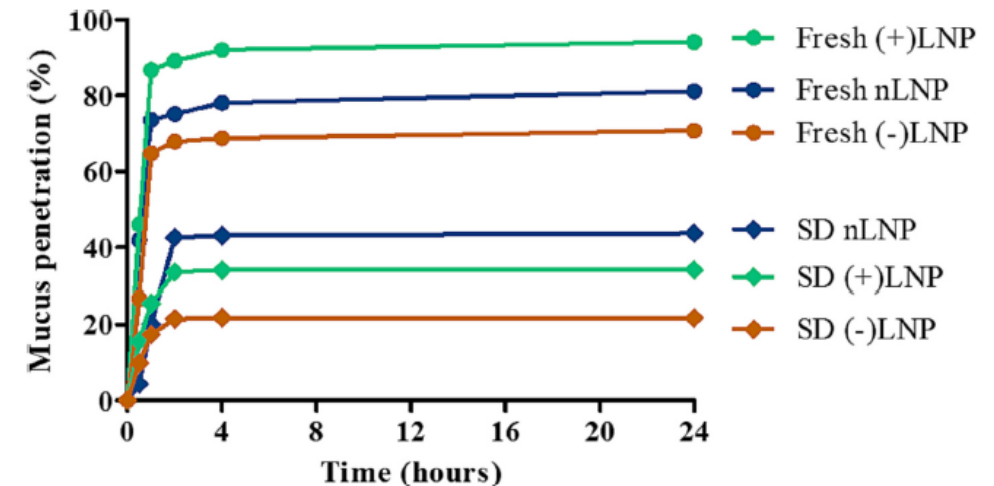
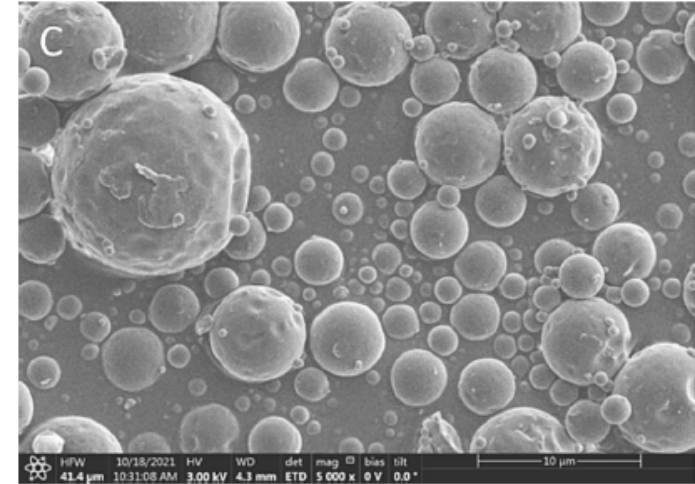
- Coating improves FPF 2-fold
- Type of metal oxide seems to impact cell viability
- Release can potentially be tailored through layer thickness
- Atomic Layer Deposition seems to be a viable technique for controlled pulmonary delivery

sample	loading (wt %)	ALD time (h)	t50 in vitro (min)	FPF (%)	cell viability (%)
uncoated budesonide	100		12.3	29.4	98.7 ± 4.6
SiO_2 / budesonide	6 nm	95.9	9.4	16.7	68.3
	10 nm	93.2	18.8	27.0	58.4
TiO_2 / budesonide	3 nm	96.2	1.9	15.0	56.8
	8 nm	89.3	4.8	21.8	52.8
Al_2O_3 / budesonide	15 nm	78.9	9.6	29.5	36.7
	20 nm	93.9	2	36.1	68.1
	35 nm	85.6	5	52.6	53.0
	50 nm	81.3	10	61.6	30.3



Spray Drying of Lipid NP for Inhalation – siRNA

- **Formulation:**
 - siGFP, Ionizable cationic lipid (analog of DLin-MC3-DMA), Cholesterol, PEG-DMG, Lactose
 - Particle size = ~150 nm
- **Spray drying at Buchi B-290:**
 - Yield = ~65%
 - Outlet temperature = 62°C and 72°C (deg.)
 - Particle size similar before/after SD
 - Moisture content = 3-4 wt.%
 - MMAD = 2.9 μm
 - Fine Particle Fraction = 28%
- Spray dried LNPs penetrated lung mucus
- Bioactivity with 90% protein downregulation
- 50% gene silencing of GADPH



Spray Drying of Lipid NP for Inhalation – mRNA

• Formulation:

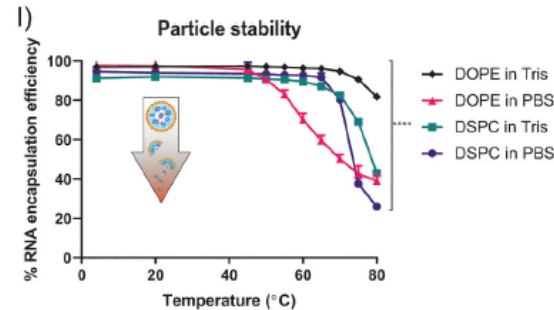
- eGFP, DSPC, DOPE, 3060i10 (Cationic lipid), Trehalose, TriLeucine
- Particle size = <200 nm

• Spray drying at Buchi B-290:

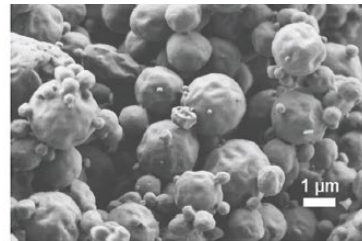
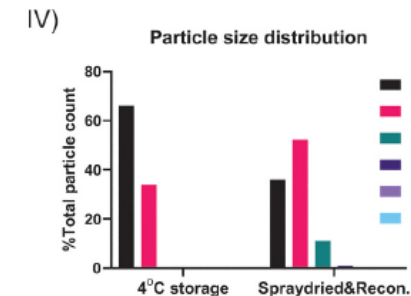
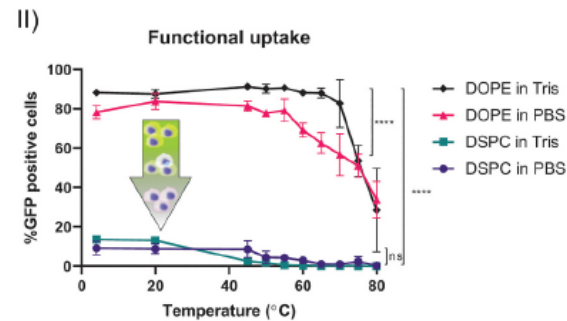
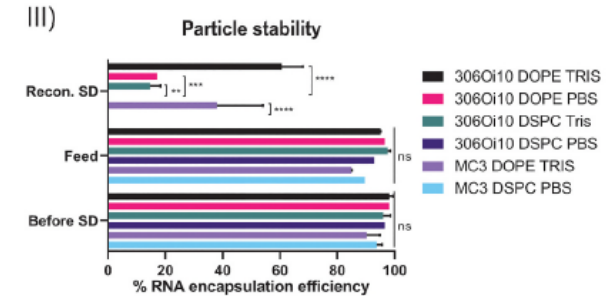
- Yield >80%
- Encapsulation Efficiency $\geq 90\%$
- Temperature (In/Out) = 90°C/54°C

- New LNP formulation was stable at higher temperatures and had higher encapsulation efficiency

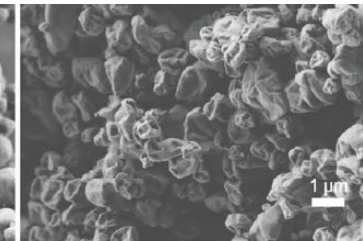
A Temperature sensitivity



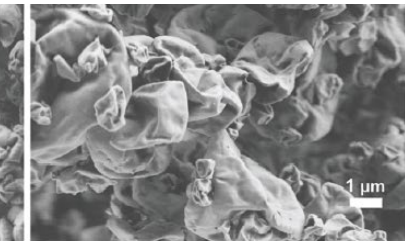
B Spray drying and reconstitution



1.5% LNP 3% LLL
12.6%EE



3% LNP 8% LLL
89.0%EE



3% LNP 15% LLL
90.2%EE

Spray Dried Particle Properties – Towards Understanding the Structure

Going from bulk properties towards resolution on particle level

- Use of imaging techniques like FIB-SEM, XRM and MFV-SEM
- Application of ML/AI algorithms to images to characterize properties like particle size, surface area, pore size distribution, chemical composition, wall/shell thickness, etc.
- Enables quantification of spray dried particle morphology in spheres vs. raisins/shrivalled fractions
 - Spheres: Low density and good compressibility
 - Raisins: High density and lower compressibility
- Potential tool to better understand how to protect sensitive molecules during spray drying through increased knowledge of component distribution and particle structure

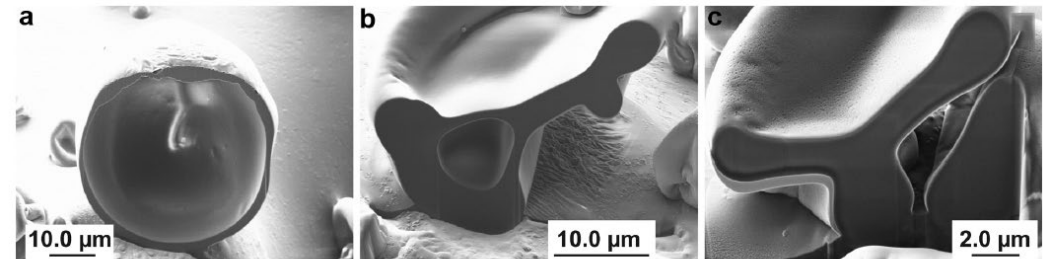
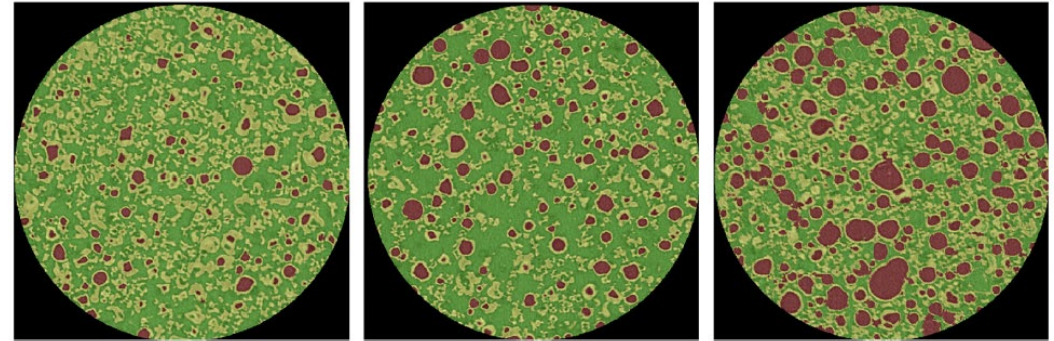


Fig. 2. FIB-SEM reveals the cross-section of MK-A SDP with different morphologies: (a) Sphere; (b) Raisin-like particle; (c) Small solid particle.

Summary/Conclusions

Image: Multiple myeloma illustration

Credit: Johnson & Johnson

Summary/Conclusions

- Biopharmaceuticals are sensitive to formulation and drying conditions:
 - Thermal stress through the drying temperature, equipment scale, shear stress, choice of solid lipid (T_m), and wall/matrix-former
- Several Spray- and Freeze-Drying based technologies are feasible for manufacturing inhalable biopharmaceuticals; Alternative technologies for „formulation“ like Atomic Layer Deposition are being researched
- Inhalation is seen as a viable route for biopharmaceuticals with multiple studies having demonstrated the feasibility for example for siRNA/mRNA
- New characterization techniques are becoming available to give new insights into particle properties
- **Production of biopharmaceuticals for inhalation by Spray -Drying and Freeze-Drying is feasible, however, still require significant formulation development work and optimization of drying conditions**

Thank you!